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(54) Abstract Title

An apparatus and method for evaluating skin health

(57) An apparatus and method for evaluating the water permeability through the stratum corneum epidermis and/or water supplying capability of a structure which lies below the stratum corneum epidermidis and is formed of living cells by using a water transpiration amount, which comprises means for feeding, from a gas inlet, a carrier gas having certain properties to a skin surface to be measured; means for measuring, by a humidity sensor, humidity of the carrier gas which has been discharged from a gas exhaust, passing over the skin surface to be measured; and means for calculating the water transpiration amount in accordance with a response to the sensor and calculating, by a predetermined analyzing method, an overall mass transfer coefficient of water in the stratum corneum epidermis and/or water vapor partial pressure of the structure which lies below the stratum corneum epidermidis and is formed of living cells.

FIG. 1

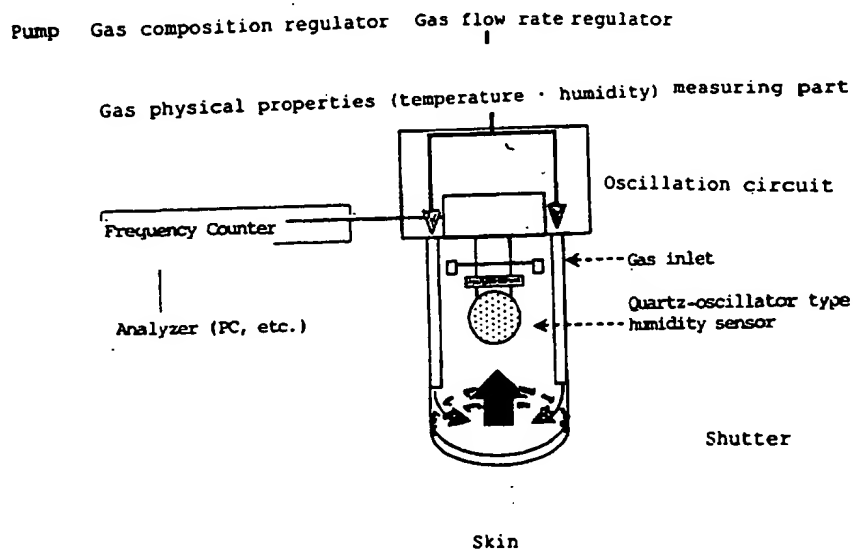


FIG. 1

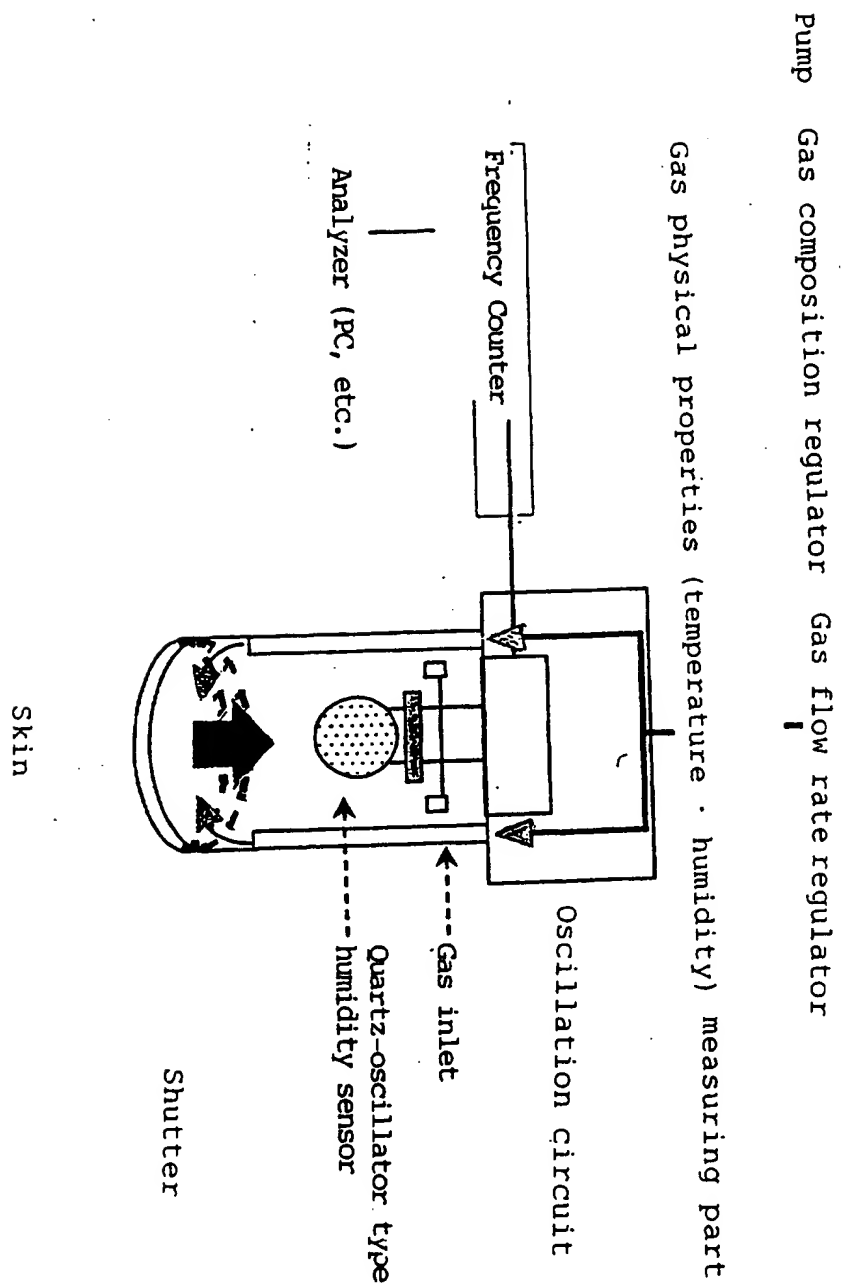
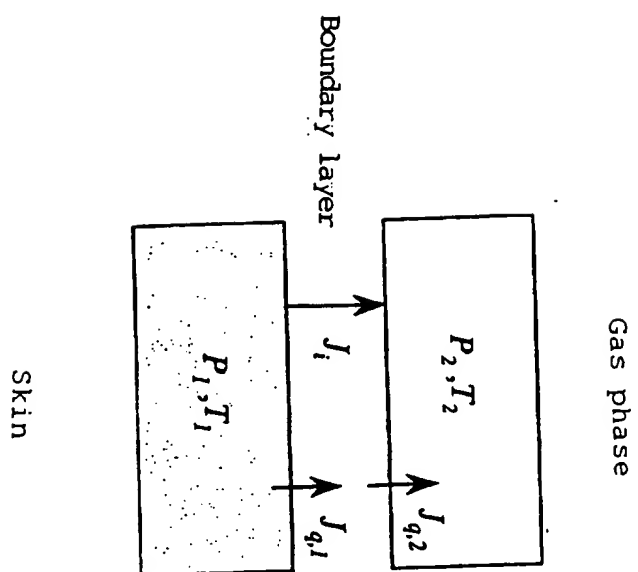


FIG. 2



T : temperature (K)
 J_i : Flux of substance (water) ($\text{g}/\text{m}^2 \cdot \text{sec}$)
 J_q : Heat flux ($\text{J}/\text{m}^2 \cdot \text{sec}$)

FIG. 3

Measuring chamber

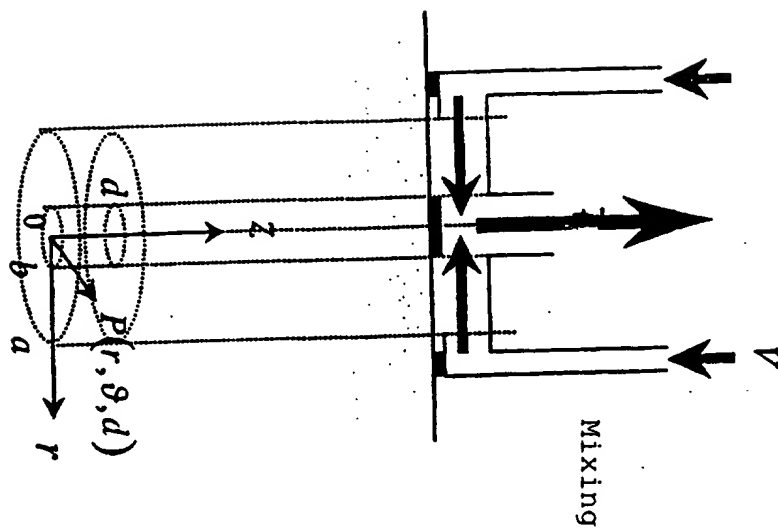
 a : Outer diameter of cell [m] b : Inner diameter of cell [m] d : Height of cell [m] P : Water vapor partial pressure V : Gas flow rate [m³/sec]

FIG. 4

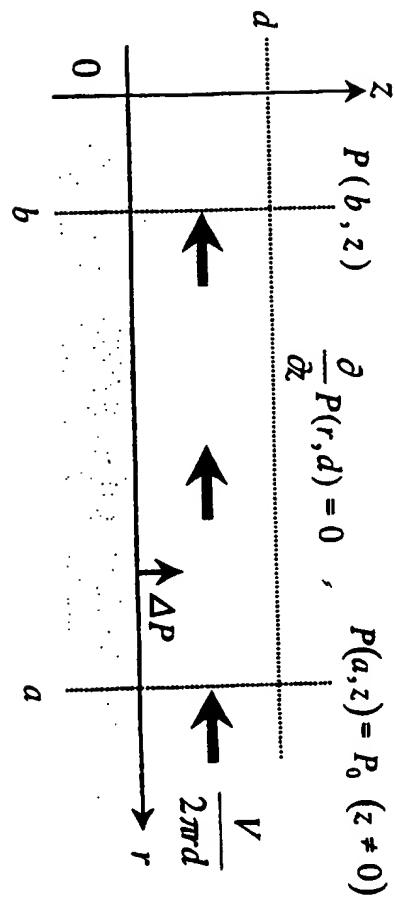
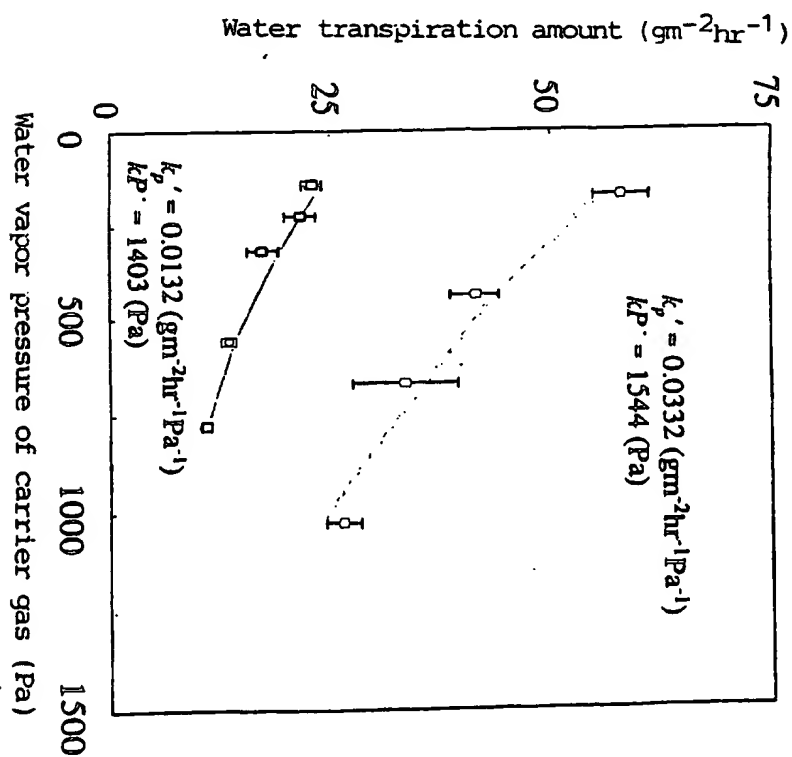
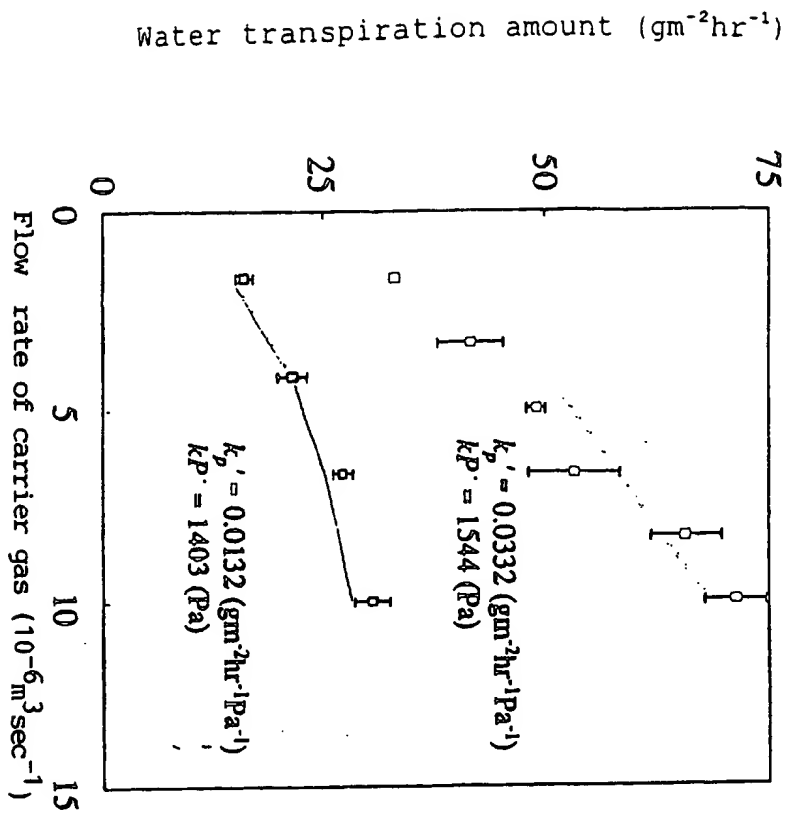


FIG. 5



Measured: Calculated:

Normal volunteer (26-year-old female) \square —

Volunteer with low-barrier skin (26-year-old female) \square ----

FIG. 6

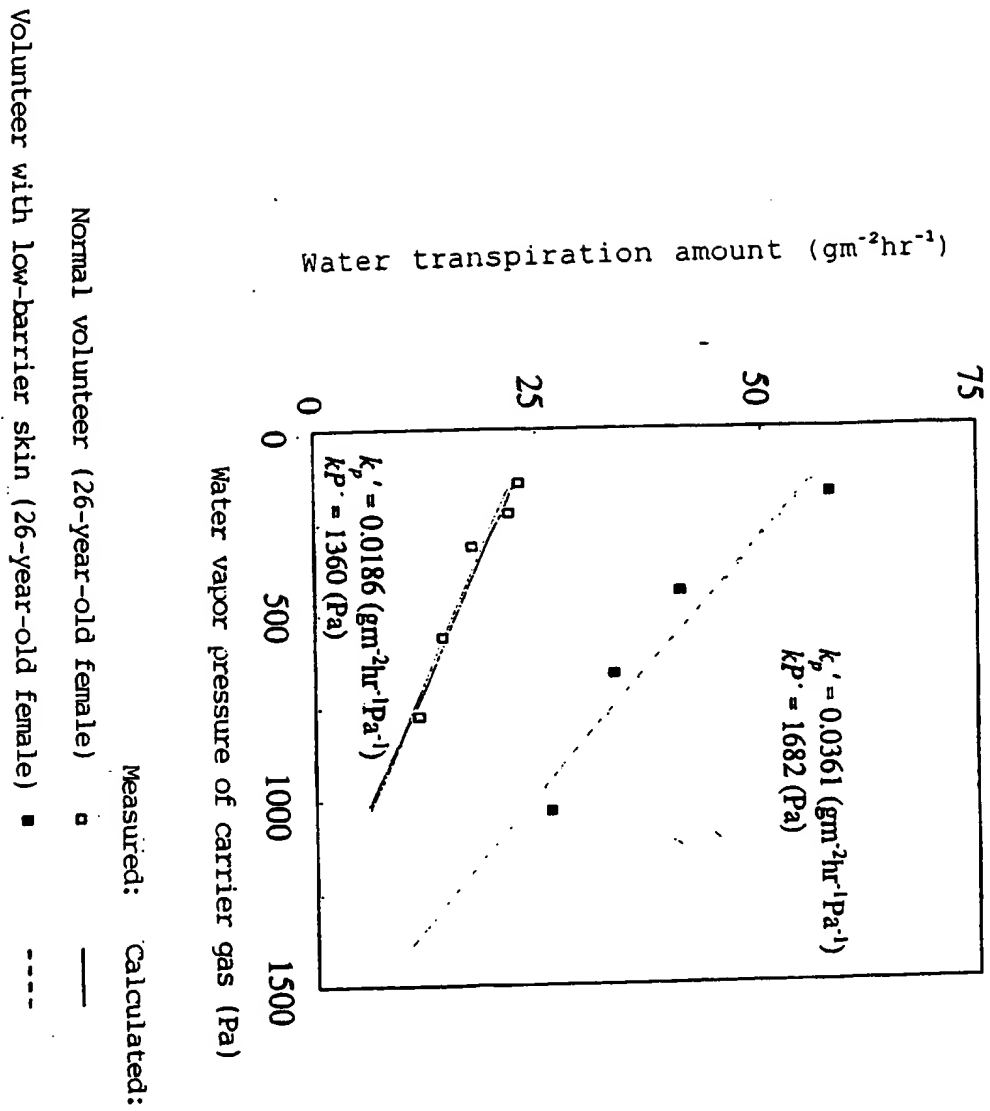


FIG. 7

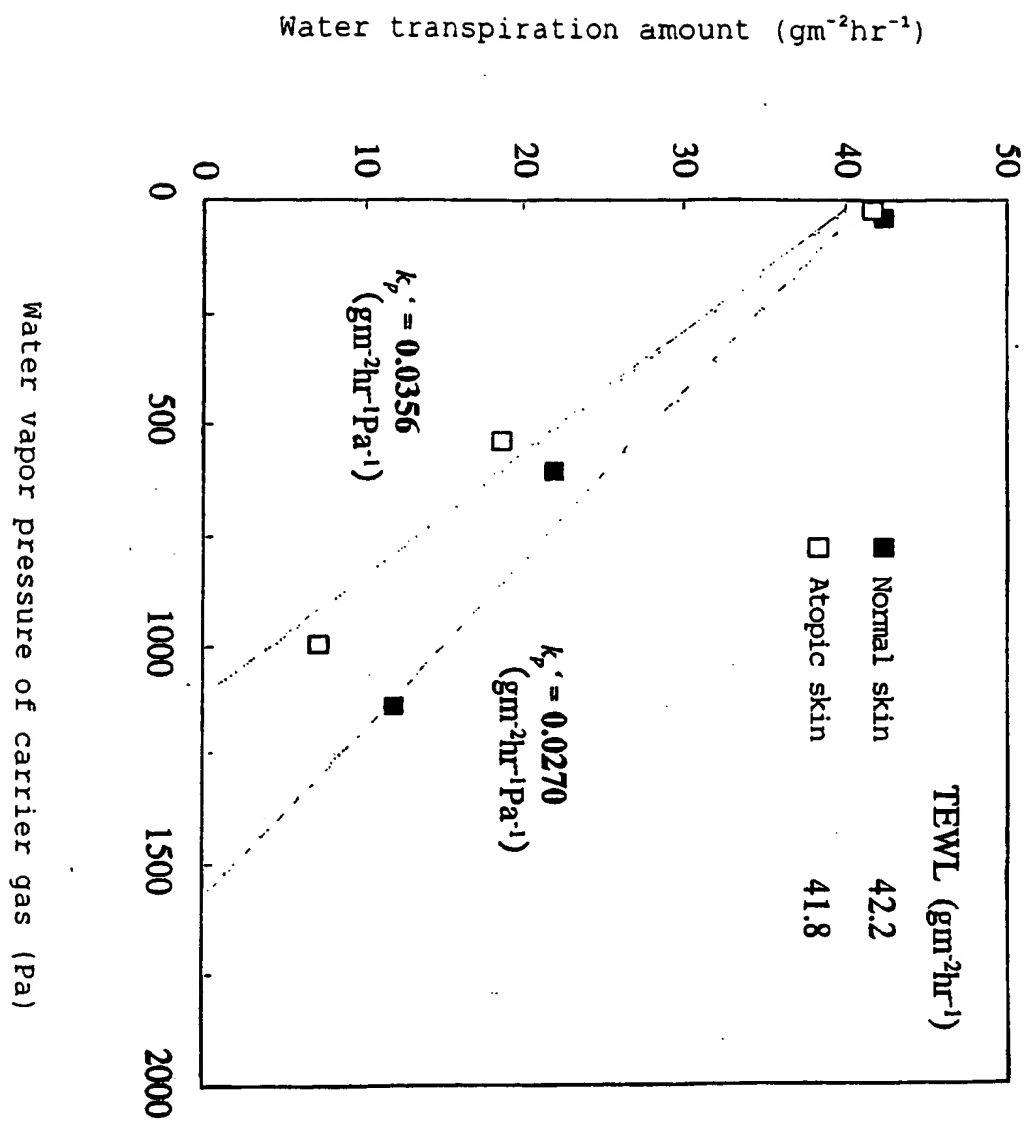
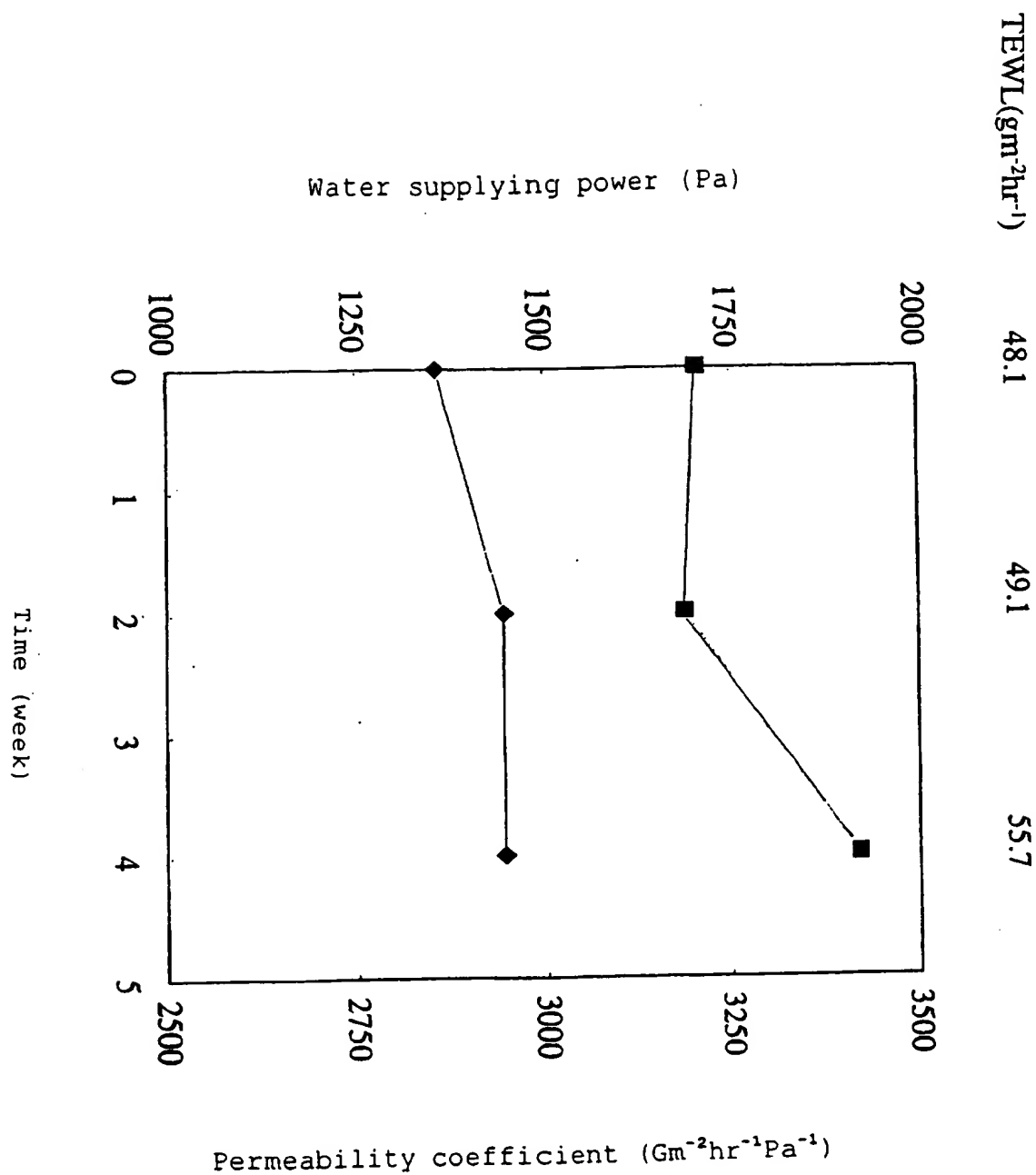


FIG. 8



METHOD FOR EVALUATING SKIN HEALTH

BACKGROUND OF THE INVENTION

1. Field of the Invention

5 The present invention relates to a method for evaluating skin health and an apparatus used therefor.

2. Description of the Related Art

 A living body always exchanges a substance and energy with an environment under which the living body exists and it has various functions of adjusting the transport amount or exchange amount of the substance or energy in accordance with an environmental change. Above all, a function of restraining transpiration of water from the skin surface, thereby protecting the living body from drying is called a barrier function and it is medically important. As an index of the barrier function, a water transpiration amount from the skin or a transepidermal water loss (TEWL) has been used widely. In the conventional method, investigation on a response of the physical properties of the skin to the environment must be carried out while changing the environment in a laboratory. It is utterly unfeasible, because a large-scaled apparatus and much labor and time are required.

25 SUMMARY OF THE INVENTION

 The present inventors paid attention to the fact that conventionally, investigation of the TEWL of the skin

included only that of the stratum corneum epidermidis but living cells therebelow were not taken into consideration. According to the conventional way of thinking, an increase in TEWL owed to deterioration in the barrier function of
5 the stratum corneum epidermidis. An increase in TEWL, however, is sometimes caused by abnormalities in the living cells below the normal stratum corneum epidermidis, and in such a case, correct diagnosis cannot be conducted.

The present inventors therefore classified the
10 structure of the skin into the stratum corneum epidermidis and living cells therebelow and considered that TEWL might be influenced not only by the water permeability through the stratum corneum epidermidis but also by a difference (driving force) in the activity of water (or water vapor
15 partial pressure) between the structure formed of living cells present below the stratum corneum epidermidis and the outside world. It is presumed that the activity of water in the living cells below the stratum corneum epidermidis reflects the concentration or composition of water and also
20 bio-reaction so that it varies depending on the properties or disease of the skin, metabolism or even age. As described above, the present inventors have found that it is important, for appropriate skin care based on not only the working degree of a barrier function but also the
25 properties or disease of the skin, metabolism or bio-reaction, to evaluate water permeability (overall mass transfer coefficient) through the stratum corneum

epidermidis and water supplying capability (activity or water vapor partial pressure) in the living cells below the stratum corneum epidermidis separately from the water transpiration amount measured by using a specified
5 apparatus. The present inventors have also found that the use of these evaluations in combination as an objective index of skin health makes it possible to conduct skin care in accordance with the skin health of each subject.

In one aspect of the present invention, there is thus
10 provided a method for evaluating water permeability through the stratum corneum epidermidis based on a water transpiration amount, which comprises feeding, through a gas inlet, a carrier gas having certain properties to a skin surface to be measured; measuring, by a humidity
15 sensor, the humidity of the carrier gas which has been discharged from a gas exhaust, passing over the skin surface to be measured; and calculating the water transpiration amount from the response of the sensor and calculating, by a predetermined analyzing method, an
20 overall mass transfer coefficient of water in the stratum corneum epidermidis; and an apparatus used for the above-described method.

In another aspect of the present invention, there is also provided a method for evaluating, based on a water
25 transpiration amount, water supplying capability of a structure which lies below the stratum corneum epidermidis and is formed of living cells, which comprises feeding,

through a gas inlet, a carrier gas having certain
properties to a skin surface to be measured; measuring, by
a humidity sensor, the humidity of the carrier gas which
has been discharged from a gas exhaust, passing over the
5 skin surface to be measured; and calculating the water
transpiration amount from the response of the sensor and
calculating, by a predetermined analyzing method, a water
vapor partial pressure of the structure which lies below
the stratum corneum epidermidis and is formed of living
10 cells; and an apparatus used for the above-described
method.

In a further aspect of the present invention, there is
also provided a method for evaluating skin health based on
a water transpiration amount, which comprises feeding,
15 through a gas inlet, a carrier gas having certain
properties to a skin surface to be measured; measuring, by
a humidity sensor, the humidity of the carrier gas which
has been discharged from a gas exhaust, passing over the
skin surface to be measured; and calculating the water
20 transpiration amount based on the response of the sensor
and calculating both an overall mass transfer coefficient
of water in the stratum corneum epidermidis and a water
vapor partial pressure of a structure which lies below the
stratum corneum epidermidis and is formed of living cells
25 by employing a predetermined analyzing method.

The terms "water permeability through the stratum
corneum epidermidis", "overall mass transfer coefficient of

the stratum corneum epidermidis", "water vapor partial pressure of a (the) structure which lies below the stratum corneum epidermidis and is formed of living cells" and "water supplying capability of a (the) structure which lies
5 below the stratum corneum epidermidis and is formed of living cells" may be replaced with the simple terms "water permeability", "overall mass transfer coefficient", "water vapor partial pressure", and "water supplying capability", respectively.

10 According to the present invention, it is possible to evaluate water permeability and water supplying capability separately by analyzing the measured value of a water transpiration amount in different manners, and employ them as an index for a barrier function, skin conditions or
15 disease, metabolism or bio-reaction. In addition, it is possible to use them in combination as an objective index of the skin health.

BRIEF DESCRIPTION OF THE DRAWINGS

20 FIG. 1 is a schematic view illustrating a skin-health-evaluating apparatus according to the present invention; FIG. 2 illustrates the model of a mass and heat exchange between the atmosphere and the skin; FIG. 3 is a cross-sectional view illustrating a measuring cell: FIG. 4 is a
25 schematic view illustrating the measuring part of a water transpiration amount (the upper portion illustrates the cross-section of the cylindrical body, while the lower

portion illustrates the circular cylindrical coordinates);
FIG. 5 illustrates water permeability and water supplying
capability as measured at varied flow rates and water vapor
partial pressures of a carrier gas: FIG. 6 illustrates
5 water permeability and water supplying capability as
measured only at varied water vapor partial pressures of a
carrier gas; FIG. 7 illustrates variations in a water
transpiration amount from each of the healthy skin and
atopic skin due to a change in water vapor partial pressure
10 of a carrier gas; and FIG. 8 illustrates variations of
water permeability and water supplying capability with the
passage of time.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

15 The apparatus for evaluating water permeability and/or
water supplying capability according to the present
invention is equipped with (1) means for feeding, from a
gas inlet, a carrier gas having certain properties to a
skin surface to be measured, (2) means for measuring the
20 humidity of the carrier gas, which has passed over the skin
surface to be measured and has then been discharged from a
gas exhaust, by a humidity sensor, and (3) means for
calculating a water transpiration amount based on the
response of the sensor, thereby calculating an overall mass
25 transfer coefficient and/or water vapor partial pressure by
a predetermined analyzing method.

The apparatus of the present invention is

schematically illustrated in FIG. 1.

Described specifically, the apparatus is, for example, formed of a cylindrical body having inside thereof a humidity sensor, an opening at each of the top and bottom
5 portion, a gas inlet on the side wall portion for feeding a gas having a fixed water content to a surface to be measured, and a freely openable or closable shutter portion at the bottom opening portion.

No particular limitation is imposed on the shape of
10 the cylindrical body insofar as it has an opening portion at the top and bottom thereof. It may have a circular cylindrical shape, prismatic shape or the like. Concerning its size, a cylindrical body having a bottom opening area of about 0.2 to 10 cm² and a height of about 2 to 20 cm is
15 preferred.

As the gas inlet, that embedded in the side wall portion of the cylindrical body may be used insofar as it is capable of feeding a certain carrier gas to a skin surface to be measured. That formed by fixing the desired
20 number of pipes, each having a nozzle hole which opens downward, to a position slightly above the end of the bottom opening portion of the cylindrical body is convenient. As the carrier gas having certain properties, that having a predetermined temperature and humidity may be
25 used and examples include dry nitrogen and dry air.

It does not matter whether the shutter portion has any structure, for example, whether it has the opening/closing

shutter mechanism of a camera or not, insofar as the bottom opening portion of the cylindrical body can be opened or closed as needed. A shutter having, at the lower part of the cylindrical body, a rotary slide plate disposed
5 pivotally for opening or closing the bottom opening portion, or is made of a valve for opening or closing the bottom opening portion by the vertical movement is simple in structure and has excellent operability.

The temperature sensor is preferably disposed above
10 the gas ejection port inside of the cylindrical body, which makes it possible to obtain a more stable and reliable measuring data. Any kind of a humidity sensor can be used, but use of a quartz oscillator humidity sensor is advantageous from the viewpoint of measuring accuracy.

15 Calculation of a water transpiration amount based on the response to the humidity sensor and then, calculation of an overall mass transfer coefficient and/or water vapor partial pressure through a predetermined analyzing method are conducted making use of an analyzer such as personal
20 computer.

The water transpiration amount (J) is calculated as described below.

A water transpiration amount J (g/m²·sec) from the skin can be expressed by the following equation:

25
$$J = \frac{1}{A} \frac{\Delta H}{100} \rho V$$

wherein, a change in relative humidity due to water

transpiration from the skin which has been found from the response to a humidity sensor is ΔH (%), a water content of the air having 100% RH at a given temperature is ρ (g/cm³), a flow rate of a carrier gas is V (m³/sec) and an area measured is A (m²).

The overall mass transfer coefficient is calculated, in accordance with Fick's diffusion relation represented by the below-described Equation 1, from at least one parameter determined using at least one measuring result of a water transpiration amount obtained by measurement with variable micro-climates of the cell while changing the flow rate, water vapor partial pressure or temperature of a carrier gas. The greater the overall mass transfer coefficient, the higher water permeability through the stratum corneum epidermidis. The smaller the overall mass transfer coefficient, the lower water permeability through the stratum corneum epidermidis.

$$J = \frac{K_m D}{\delta} (C_d - C_r) \quad \text{Equation 1}$$

wherein, K_m is a partition coefficient, D represents a diffusion coefficient (m²/sec), δ represents the thickness (m) of the stratum corneum epidermidis, and C_d and C_r represent the water concentrations (kg/m³) of the water doner side and water receiver side, respectively.

More specifically, the overall mass transfer coefficient can be calculated using either one of the

below-described analytical method (1) or (2).

(1) An overall mass transfer coefficient k_p' ($\text{g/m}^2 \cdot \text{sec}$ or $\text{g/m}^2 \cdot \text{sec} \cdot \text{Pa}$) is determined by calculating the parameter K using the value of at least one water transpiration
5 amount measured by changing the flow rate, water vapor partial pressure or temperature of a carrier gas and the value calculated in accordance with the below-described Equations 8 and 9, followed by calculation in accordance with the below-described Equation 2 using the resulting
10 parameter K .

$$k_p' = dK\rho \frac{M_{\text{H}_2\text{O}}}{M_{\text{gas}}} \quad \text{Equation 2}$$

wherein, ρ represents the gas density (g/m^3), and M
15 represents a molecular weight.

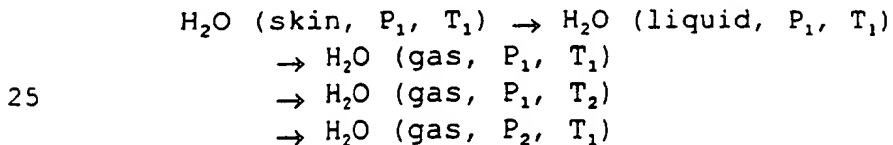
Such measurement with variable micro-climates of the cell can be conducted by changing any one of the flow rate, water vapor partial pressure and temperature of a carrier gas, of which the former two is preferred. In particular,
20 measurement conducted changing both of the flow rate and water vapor partial pressure of a carrier gas is preferred, because it brings about highly-accurate evaluation results.

(2) The overall mass transfer coefficient is calculated in accordance with the below-described Equation
25 11 based on the measured values obtained by changing the water vapor pressure of at least two carrier gases.

Equations 2, 8, 9 and 11 are introduced from a model made as follows:

The atmosphere/skin system in which water transpiration is occurring is not a static system. Water transpiration from the skin is evidently a steady state and it is an irreversible process.

5 The atmosphere/skin system is supposed as an ideal system wherein heat and mass are transported through a thin layer (barrier layer) sandwiched between two pseudo-infinite phases having a predetermined temperature and composition (FIG. 2). The barrier layer is a layer highly
10 resistant against the transfer of the mass and may exist on the side of the skin in this system. The bulk has uniform properties in each of the skin and gas phase and the changing rate of their properties are sufficiently low (so low that it can be regarded as changeless) relative to a
15 time scale discussed here. The flux of each of heat and mass is strictly one-dimensional and vertical to the barrier layer and a gradient between two phases in temperature or chemical composition exists only on the barrier layer. The gas phase behaves as an ideal gas. For
20 introduction of an analysis equation, a reversible path to the transportation of water from the skin to the atmosphere as described below is supposed.



(A) Introduction of an analysis equation of the transportation rate and direction of water which has passed

through the atmosphere/skin interface

In accordance with the thermodynamic method based on an irreversible process, the below-described Equation 3 for analyzing the flux J_i of water which has passed through the atmosphere/skin interface is introduced.

$$J_i = \frac{dP}{dt} = \frac{KP_m}{RT_m} \left(q^* \frac{T_2 - T_1}{T_m} + RT_m \ln \frac{kP'}{P_2} \right)$$

Equation 3

wherein, q^* represents a thermal change relating to isothermal transfer of a solute or vapor from the skin to the atmospheric layer, K stands for a rate constant (1/sec), k stands for a constant, P' stands for saturated vapor pressure, P_m stands for a mean water vapor partial pressure within a barrier layer and T_m stands for a mean temperature within a barrier layer.

(B) Introduction of an analysis equation of water vapor pressure distribution inside of the measuring cell

The shape of the cylindrical body which can be adopted here is not limited, but an analysis method will hereinafter be described using a cylindrical body which is formed to allow a carrier gas to flow along the outside wall, pass it over the surface of the skin and discharge it from the center of the cylinder. When it is assumed that the carrier gas flows along the outside wall of the cylindrical body into the inside of the cell at a flow rate of V (m^3/sec), passes over the surface of the skin and is

then discharged (FIGS. 3 and 4), the diffusion equation in this measuring system can be expressed as the following Equation 4.

$$\frac{\partial P}{\partial t} = D \frac{1}{r} \frac{\partial}{\partial r} \left(r \frac{\partial P}{\partial r} \right) + \frac{V}{2\pi r d} \frac{\partial P}{\partial r} + D \frac{\partial^2 P}{\partial z^2}$$

5

Equation 4

wherein, D (m^2/sec) stands for a diffusion coefficient of water into the atmospheric layer.

Under a steady state, Equation 4 is equal to 0, leading to the following Equation 5.

$$D \frac{1}{r} \frac{\partial}{\partial r} \left(r \frac{\partial P}{\partial r} \right) + \frac{V}{2\pi r d} \frac{\partial P}{\partial r} + D \frac{\partial^2 P}{\partial z^2} = 0$$

10

Equation 5

When Equation 5 is solved under the following boundary conditions:

$$\begin{cases} P(a, z) = P_0 (z \neq 0) \\ \frac{\partial}{\partial z} P(r, d) = 0 \end{cases}$$

wherein, P_0 stands for a water vapor partial pressure in the gas before the gas enters into the cell, the solution of Equation 5 is equal to Equation 6 when water vapor is generated continuously at $r = a$ to b .

$$P(b, z) = P_0 + \int_a^b \frac{dP_1}{ds} \left[1 + 2 \sum_{m=1}^{\infty} \cos\left(\frac{m\pi z}{d}\right) \right] \frac{\sum_{n=1}^{\text{even}} a_n b^n}{\sum_{n=1}^{\text{even}} a_n s^n} ds$$

$$a_0 = 1$$

$$a_n = \frac{m^2 \pi^2}{d^2 n \left(n + \frac{V}{2\pi D d} \right)} a_{n-2} \quad (n \geq 2)$$

Equation 6

(C) Introduction of an analysis equation for the measurement with variable micro-climates of the cell

The following Equation 8:

$$P(b, z) = P_0 + \int_a^b \frac{dP}{ds} \left[1 + 2 \sum_{m=1}^{\infty} \cos\left(\frac{m\pi z}{d}\right) \right] \frac{\sum_{n=1}^{\text{even}} a_n b^n}{\sum_{n=1}^{\text{even}} a_n s^n} ds$$

$$= P_0 + \int_a^b \frac{2\pi s d}{V} \frac{KP_m}{RT_m} \left[q \cdot \frac{T_2 - T_1}{T_m} + RT_m \ln \frac{kP'}{P(s, 0)} \right] \left[1 + 2 \sum_{m=1}^{\infty} \cos\left(\frac{m\pi z}{d}\right) \right] \frac{\sum_{n=1}^{\text{even}} a_n b^n}{\sum_{n=1}^{\text{even}} a_n s^n} ds$$

$$a_0 = 1$$

$$a_n = \frac{m^2 \pi^2}{d^2 n \left(n + \frac{V}{2\pi D d} \right)} a_{n-2} \quad (n \geq 2)$$

5

Equation 8

, that is, an equation for analyzing a relation between measuring conditions and a water transpiration amount is introduced by uniting the following Equation 7:

$$-\frac{dP}{dr} = \frac{dP/dt}{dr/dt} = \frac{2\pi r d}{V} \frac{KP_m}{RT_m} \left(q \cdot \frac{T_2 - T_1}{T_m} + RT_m \ln \frac{kP'}{P_2} \right)$$

Equation 7

10 available from Equation 3 for analyzing the transpiration rate of water which has passed through an atmosphere/skin interface and Equation 5 for analyzing the water vapor partial pressure distribution inside of the measuring cell.

With regards to the second member on the right side of
15 Equation 8, the contribution of this member due to a

temperature difference is within 4%, negligible small when a temperature difference (about 30K at the maximum) between the ordinary environment and inside of the living body is taken into consideration, which makes it possible to

5 introduce the following Equation 8-2:

$$P(b,z) = P_0 + \int_b^s \frac{2\pi s d}{V} K P_m \ln \frac{k P^*}{P(s,0)} \left[1 + 2 \sum_{m=1}^{\infty} \cos\left(\frac{m\pi z}{d}\right) \right] \frac{\sum_{n=0}^{\text{even}} a_n b^n}{\sum_{n=0}^{\text{even}} a_n s^n} ds$$

Equation 8-2

Here, with a system which satisfies $\Delta P \ll P_m$ (which is assumed to correspond to the atmosphere/skin system), approximation represented by $\ln(P_1/P_2) \cong \Delta P/P_m$ is conducted,

10 whereby the following Equation 8-3 is introduced:

$$P(b,z) = P_0 + \int_b^s \frac{2\pi s d}{V} K [k P^* - P(s,0)] \left[1 + 2 \sum_{m=1}^{\infty} \cos\left(\frac{m\pi z}{d}\right) \right] \frac{\sum_{n=0}^{\text{even}} a_n b^n}{\sum_{n=0}^{\text{even}} a_n s^n} ds$$

Equation 8-3

For analysis of measurements with variable micro-climates of the cell, Equation 8-2 or 8-3 may be used instead of Equation 8.

15 (D) Introduction of water permeability

A water transpiration amount ($\text{g/m}^2 \cdot \text{sec}$) under desired measuring conditions is calculated in accordance with the following Equation 9.

$$J = \frac{\left(\int_0^d P(b, z) dz - P_0 \right) \rho V}{\pi(a^2 - b^2)} \frac{M_{H_2O}}{M_{gas}}$$

Equation 9

wherein, ρ stands for a gas density (g/m^3) and M stands for molecular weight.

When a water vapor partial pressure inside of the measuring cell increases by ΔP per unit time owing to water vapor transpiration from the skin surface, the following Equation 10:

$$J = \frac{1}{A} \rho A d \frac{dP}{dt}$$

$$J = \frac{1}{\pi(a^2 - b^2)} \rho \frac{M_{H_2O}}{M_{gas}} \pi(a^2 - b^2) d \frac{KP_m}{RT_m} \left[q \cdot \frac{T_1 - T_2}{T_m} + RT_m \ln \frac{KP^*}{P_2} \right]$$

Equation 10

can be introduced.

This Equation 10 is separated into restraining and driving force terms. The contribution caused by a difference between a temperature under the ordinary circumstance and that inside of the living body is within 4% and its influence is negligible. With a system which satisfies $\Delta P \ll P_m$ (which is assumed to correspond to the atmosphere/skin system), approximation represented by $\ln(P_1/P_2) \cong \Delta P/P_m$ is conducted, leading to the following Equation 11:

$$J = \frac{1}{\pi(a^2 - b^2)} \rho \frac{M_{H_2O}}{M_{gas}} \pi(a^2 - b^2) d \frac{KP_m}{RT_m} \left[q \cdot \frac{T_1 - T_2}{T_m} + RT_m \ln \frac{kP'}{P_2} \right]$$

$$\approx dK\rho \frac{M_{H_2O}}{M_{gas}} \times (kP' - P_1)$$

Equation 11

and an overall mass transfer coefficient ($g/m^2 \cdot sec$ or $g/m^2 \cdot sec \cdot Pa$), which means water permeability, can be determined from the following Equation 2:

$$k_p' = dK\rho \frac{M_{H_2O}}{M_{gas}} \quad \text{Equation 2}$$

The "overall mass transfer coefficient" introduced from the measuring results of a water transpiration amount is also called mass transfer coefficient, permeability coefficient, permeation or permeability. The diffusion coefficient or diffusion properties determined from the overall mass transfer coefficient, for example, in accordance with the below-described relationship can also be used for the evaluation of water permeability.

$$k_p' = K_m \cdot D/\delta$$

wherein, k_p' stands for an overall mass transfer coefficient, K_m stands for a partition coefficient, D stands for a diffusion coefficient and δ stands for the thickness of a membrane.

Each of the terms "water permeation", "barrier function", "barrier characteristics", "barrier properties", "barrier capacity" and "water loss suppressing power" has

the same meaning as the term "water permeability" through the stratum corneum epidermidis evaluated using an overall mass transfer coefficient introduced from the measuring results of a water transpiration amount and they can be
5 used similarly.

(E) Introduction of water supplying capability

The term "water supplying capability" as used herein means a water vapor partial pressure in a structure which lies below the stratum corneum epidermidis and is formed of
10 living cells. The water supplying capability corresponds to kP' in Equation 3 which is available as a result of analysis of measurement with variable micro-climates of the cell using Equation 8, 8-2 or 8-3. According to Equation 11, when the activity of water (water vapor partial
15 pressure) contained in a gas phase or a carrier gas is equal to that of a structure which lies below the stratum corneum epidermidis and is formed of living cells, a water transpiration amount (J) should become 0. It is therefore possible to apply Equation 11 to a change of a water
20 transpiration amount due to a water vapor partial pressure of a gas phase or a carrier gas, thereby determining, as the value of the intercept x , a water vapor partial pressure, that is, water supplying capability, in a structure which lies below the stratum corneum epidermidis
25 and is formed of living cells.

The "water vapor partial pressure" introduced from the measuring results of a water transpiration amount is also

called "water vapor pressure", "vapor pressure of water" or "fugacity" and "water content", "concentration of water", "activity" or "water vapor amount" determined from the water vapor partial pressure can also be used for the evaluation of water supplying capability. The concentration of water can be found, for example, by the following relationship:

$$P = H \cdot C$$

wherein, P stands for a water vapor partial pressure, H represents a constant and C represents the concentration of water.

Each of the terms "power for promoting water transpiration", "water content", "activity", "moisturized feeling" and "concentration of water" has the same meaning as the term "water supplying capability" introduced from the measuring results of a water transpiration amount and they can be used similarly.

As described above, "water permeability" evaluated in the present invention represents the function of the stratum corneum, while "water supplying capability" represents the function of a structure which lies below the stratum corneum epidermidis and is formed of living cells. The skin health (including the stratum corneum and living cells therebelow) can be evaluated totally by the evaluation of these two factors.

For example, when no change is observed from the living cells below the stratum corneum and an abnormality

exists only in the stratum corneum, only water permeability shows an abnormal value. When not the stratum corneum but the living cells therebelow are abnormal, on the other hand, only water supplying capability becomes abnormal. It is of course possible to diagnose the case where both are abnormal.

Examples

Example 1

Evaluation results of the water permeability and water supplying capability of a normal volunteer (26-year-old female) and a volunteer (26-year-old female) with low-barrier-skin at their cheek portion will next be described.

(1) Evaluation method 1

In FIG. 5, illustrated are overall mass transfer coefficient k_p' (that is, water permeability) and water vapor partial pressure kP' (that is, water supplying capability) calculated from K, k determined by fitting the values measured by changing the flow rate and water vapor pressure of a carrier gas and the values calculated according to Equations 8 and 9. The water permeabilities of the normal volunteer and volunteer with low-barrier-skin were 0.0132 and 0.0332 ($\text{gm}^{-2}\text{hr}^{-1}\text{Pa}^{-1}$), respectively. Their water supplying capabilities were 1544 and 1403 (Pa), respectively.

(2) Evaluation method 2

In FIG. 6, illustrated are water permeability and water supplying capability calculated based on Equation 11

from the value measured by changing the water vapor partial pressure of a carrier gas. The water permeabilities of the normal volunteer and volunteer with low-barrier-skin were 0.0186 and 0.0361 ($\text{gm}^{-2}\text{hr}^{-1}\text{Pa}^{-1}$), respectively. Their water
5 supplying capabilities were 1360 and 1682 (Pa), respectively.

Comparison between FIG. 5 and FIG. 6 indicates that the accuracy of the former evaluation method is high, however, the latter one which is inferior in accuracy to
10 the former one can also be employed as a method for evaluation of both of water permeability and water supplying capability.

Example 2

Evaluation results of the water permeability and water
15 supplying capability of Volunteer A (36-year-old female with normal skin) and Volunteer B (32-year-old female with atopic skin) at their cheek portion will next be described.

Water permeability calculated, in accordance with Equation 11, from the values measured at varied water vapor
20 partial pressures of a carrier gas is illustrated in FIG. 7. The TEWL (extrapolated value when the humidity of a carrier gas is 0%RH) and water permeability of Volunteer A and Volunteer B were 41.4 and 40.9 ($\text{gm}^{-2}\text{hr}^{-1}$), and 0.0270 and 0.0356 ($\text{gm}^{-2}\text{hr}^{-1}\text{Pa}^{-1}$), respectively, suggesting that the
25 water permeability of Volunteer B was greater than that of Volunteer A in spite that they were almost similar in TEWL. According to the conventional evaluation based on the value

of TEWL, they were regarded to have an equal barrier function. When water permeability is employed as an index, on the other hand, the barrier function can be evaluated more precisely, reflecting the actual skin state.

5 Example 3

Evaluation results of water permeability and water supplying capability of a normal volunteer (31-year-old female) at her cheek portion with the passage of time, more specifically, after 0, 2 and 4 weeks, will next be
10 described.

Changes in each of water permeability and water supplying capability after 0, 2 and 4 weeks which were calculated, in accordance with Equation 11, from the values measured at varied water vapor partial pressures of a
15 carrier gas are shown in FIG. 8. The TEWLs after 0, 2 and 4 weeks were 48.1, 49.1 and 55.7 ($\text{gm}^2\text{hr}^{-1}$), respectively. FIG. 8 indicates that the water permeability showed almost no change from 0 to 4 weeks, while the water supplying capability showed a drastic increase at the fourth week.
20 As a result of diagnosis by a doctor, the skin condition was substantially the same for those four weeks, while as a result of questionnaire, the physical condition of the volunteer was bad owing to the worsening of pollinosis from the second week to the fourth week. Although it was
25 conventionally impossible to measure a change in the physical condition, at least a change in the physical condition by pollinosis was grasped by using the water

supplying capability as an evaluation index.

What is claimed is:

1. An apparatus for evaluating water permeability through the stratum corneum epidermidis by using a water transpiration amount, which comprises means for feeding, through a gas inlet, a carrier gas having certain properties to a skin surface to be measured; means for measuring, by a humidity sensor, the humidity of the carrier gas which has been discharged from a gas exhaust, passing over the skin surface to be measured; and means for calculating the water transpiration amount in accordance with a response to the sensor and calculating, by a predetermined analyzing method, an overall mass transfer coefficient of water in the stratum corneum epidermidis.

2. A method for evaluating water permeability through the stratum corneum epidermidis by using a water transpiration amount, which comprises feeding, through a gas inlet, a carrier gas having certain properties to a skin surface to be measured; measuring, by a humidity sensor, the humidity of the carrier gas which has been discharged from a gas exhaust, passing over the skin surface to be measured; and calculating the water transpiration amount in accordance with a response to the sensor and calculating, by a predetermined analyzing method, an overall mass transfer coefficient of water in the stratum corneum epidermidis.

3. An apparatus for evaluating water supplying capability of a structure which lies below the stratum

corneum epidermidis and is formed of living cells by using
a water transpiration amount, which comprises means for
feeding, from a gas inlet, a carrier gas having certain
properties to a skin surface to be measured; means for
5 measuring, by a humidity sensor, humidity of the carrier
gas which has been discharged from a gas exhaust, passing
over the skin surface to be measured; and means for
calculating the water transpiration amount in accordance
with a response to the sensor and calculating, by a
10 predetermined analyzing method, a water vapor partial
pressure of the structure which lies below the stratum
corneum epidermidis and is formed of living cells.

4. A method for evaluating water supplying capability
of a structure which lies below the stratum corneum
15 epidermidis and is formed of living cells by using a water
transpiration amount, which comprises means for feeding,
through a gas inlet, a carrier gas having certain
properties to a skin surface to be measured; means for
measuring, by a humidity sensor, humidity of the carrier
20 gas which has been discharged from a gas exhaust, passing
over the skin surface to be measured; and means for
calculating the water transpiration amount in accordance
with a response to the sensor and calculating, by a
predetermined analyzing method, a water vapor partial
25 pressure of the structure which lies below the stratum
corneum epidermidis and is formed of living cells.

5. A method for evaluating the skin health by using a

water transpiration amount, which comprises feeding,
through a gas inlet, a carrier gas having certain
properties to a skin surface to be measured; measuring, by
a humidity sensor, humidity of the carrier gas which has
5 been discharged from a gas exhaust, passing over the skin
surface to be measured; and calculating the water
transpiration amount based on a response to the sensor and
calculating an overall mass transfer coefficient of water
in the stratum corneum epidermidis and water vapor partial
10 pressure of the structure which lies below the stratum
corneum epidermidis and is formed of living cells.



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Databases searched:

UK Patent Office collections, including GB, EP, WO & US patent specifications, in:

UK CI (Ed.S): G1N (NENX, NEND, NACL)

Int CI (Ed.7): A61B (5/103 5/00) G01N (27/00)

Other: Online: WPI, EPODOC, JAPIO

Documents considered to be relevant:

Category	Identity of document and relevant passage	Relevant to claims
X	US 5131390 A KAMEI Figures 1, 3 & 4 and the abstract	1 & 2
X	WPI Abstract Accession No. 1988-095519 & JP 630046131A (Suzuken) 27.02.88 (see abstract)	1 & 2

X	Document indicating lack of novelty or inventive step	A	Document indicating technological background and/or state of the art.
Y	Document indicating lack of inventive step if combined with one or more other documents of same category.	P	Document published on or after the declared priority date but before the filing date of this invention.
&	Member of the same patent family	E	Patent document published on or after, but with priority date earlier than, the filing date of this application.